Accepted for publication in Medicine & Science in Sports & Exercise, June 2016

Footwear matters: Influence of footwear and foot strike on loadrates during running

- 3
- 4 Hannah M. Rice, PhD^{1,2}
- 5 Steve T. Jamison, PhD¹
- 6 Irene S. Davis, PhD, PT, FACSM, FAPTA, FASB¹
- Spaulding National Running Center, Department of Physical Medicine and Rehabilitation, Harvard Medical School, Cambridge, MA, 02138, USA.
- Sport and Health Sciences, College of Life and Environmental Sciences, St. Luke's Campus, University of Exeter, Heavitree Road, Exeter, Devon, EX1 2LU, UK.
- 12

9

- 13 Corresponding Author:
- 14 Hannah Rice, PhD

Sport and Health Sciences, College of Life and Environmental Sciences, St Luke's Campus,
University of Exeter, Heavitree Road, Exeter, Devon, EX1 2LU, UK.

- 17 +44 (0)1392 724722
- 18 H.Rice@exeter.ac.uk
- 19
- 20
- This is a non-final version of an article published in final form in Medicine and Science in Sports and Exercise, 2016 Jul 6.

Accepted for publication in Medicine & Science in Sports & Exercise, June 2016

- 23
- 24 Abstract

Introduction: Running with a forefoot strike (FFS) pattern has been suggested to reduce the risk of overuse running injuries, due to a reduced vertical loadrate compared with rearfoot strike (RFS) running. However, resultant loadrate has been reported to be similar between foot strikes when running in traditional shoes, leading to questions regarding the value of running with a FFS. The influence of minimal footwear on the resultant loadrate has not been considered. This study aimed to compare component and resultant instantaneous loadrate (ILR) between runners with different foot strike patterns in their habitual footwear conditions.

32 **Methods:** 29 injury-free participants (22 males, 7 females) ran at 3.13m.s⁻¹ along a 30m runway,

33 with their habitual foot strike and footwear condition. Ground reaction force data were collected.

Peak ILR values were compared between three conditions; those who habitually run with a RFS
in standard shoes, with a FFS in standard shoes, and with a FFS in minimal shoes.

Results: Peak resultant, vertical, lateral and medial ILR were lower (P < 0.001) when running in minimal shoes with a FFS than in standard shoes with either foot strike. When running with a FFS, peak posterior ILR were lower (P < 0.001) in minimal than standard shoes.

39 Conclusions: When running in a standard shoe, peak resultant and component instantaneous 40 loadrates were similar between footstrike patterns. However, loadrates were lower when running 41 in minimal shoes with a FFS, compared with running in standard shoes with either foot strike. 42 Therefore, it appears that footwear alters the loadrates during running, even with similar foot 43 strike patterns.

44

45

Key Words: ground reaction force; resultant; overuse injury; minimalist; forefoot
47
48

Accepted for publication in Medicine & Science in Sports & Exercise, June 2016

49 Introduction

The relationship between foot strike pattern and injury during running has been the subject of 50 51 much discussion in recent years. This is because the vertical impact transient characteristic of a rearfoot strike (RFS) (3) is associated with a high rate of loading experienced by the body. The 52 musculoskeletal system is viscoelastic in nature and therefore sensitive to high rates of loading. 53 This was underscored by earlier animal studies that demonstrated that impulsive impact loading 54 was associated with both bony (22) and cartilaginous (23) injuries. In humans, high loadrates 55 during running have since been associated with lower extremity overuse injuries in retrospective 56 studies (17, 21, 31). A recent prospective study suggests that high loadrates can distinguish 57 58 between those who develop any medically diagnosed running-related injury, and those who have never been injured, further strengthening this relationship (8). 59

60 It has previously been reported that a forefoot strike (FFS) pattern is missing the impact transient in the vertical ground reaction force that is characteristic of a RFS pattern (15). This FFS pattern 61 has been associated with markedly lower vertical loading rates (15). In a recent study, Daoud and 62 colleagues reported that collegiate cross-country runners who habitually FFS experience fewer 63 repetitive stress running injuries compared with those who habitually RFS (7). Additionally, 64 transitioning to a FFS pattern has been reported to resolve a variety of chronic running-related 65 injuries including patellofemoral pain syndrome (4) and anterior compartment syndrome (9). 66 However, footwear was not considered in these studies. Additionally, all of these studies focused 67 only on the vertical component of the ground reaction force. 68

69 While the vertical ground reaction force is the largest component of the total ground reaction 70 force, forces in the anteroposterior (AP) and mediolateral (ML) directions also contribute to the

Accepted for publication in Medicine & Science in Sports & Exercise, June 2016

loading forces the body experiences. Yet, the resultant ground reaction force, and its associated 71 loadrate, has received little attention in the running literature. The resultant loadrate may be 72 important in terms of injury risk, as this is the total rate of loading that is applied to the body, and 73 was found to be at least as high as the vertical instantaneous loading rate (ILR) by Boyer et al. 74 (2). These authors reported that the resultant ILR was similar between habitual RFS and FFS 75 runners in standard running shoes, despite slightly lower vertical ILR when running with a FFS 76 compared with a RFS. They also found that ILR in the posterior and medial directions were 77 higher when running with a FFS than a RFS, likely due to impact peaks in these directions that 78 are characteristic of traditionally shod FFS running. These increases in posterior and medial ILR 79 may explain why the resultant ILR was similar between foot strikes. If there is no difference in 80 the total rate of loading to the body between a FFS and a RFS, it is reasonable to question the 81 overall value of FFS running. However, this similarity in resultant ILR has only been observed 82 during running in traditional, cushioned running shoes with a heel-toe drop. 83

Minimal shoes are often recommended when transitioning to a FFS pattern, as their lack of 84 cushioning discourages landing on the heel. In fact, running in minimal shoes has been shown to 85 encourage a more anterior foot strike than running in traditional shoes (20, 27). Landing on 86 stiffer surfaces has been shown to result in more compliant landings (1, 10, 16), thus running in 87 minimal shoes may have a similar influence. Running in minimal shoes has been shown to result 88 in lower vertical impact loading than running in standard shoes (27) but resultant loadrates were 89 not examined in this study. These authors also noted a more anterior foot strike in minimal shoes, 90 but comparisons to running with a FFS pattern in standard shoes were not made. It should be 91 noted that running barefoot or in minimalist footwear has been associated with stress reactions in 92 the metatarsals (11, 24, 25). However, it remains unclear whether this was the influence of 93

Accepted for publication in Medicine & Science in Sports & Exercise, June 2016

94 footwear, or was confounded by the brief transition these runners underwent. Boyer et al. (2)
95 reported that when runners were asked to transition to a novel RFS or FFS, they immediately
96 exhibited exaggerated RFS or FFS characteristics compared with the characteristics of runners in
97 their habitual group. This suggests the novel condition was not representative of the habitual
98 state and highlights the need for more ecologically valid research in which participants run in
99 their typical condition.

The aim of this study was to assess the component, as well as the resultant GRF and ILR during running in three distinct groups of runners. These groups were: those who habitually run in standard shoes with a RFS those who habitually run in standard shoes with a FFS; and those who habitually run in minimal shoes with a FFS. It was hypothesized that FFS runners would demonstrate a lower peak vertical ILR than RFS runners. It was also hypothesized that running with a FFS pattern in minimal shoes would result in lower posterior, medial and lateral ILR, and therefore a lower peak resultant ILR, than running with a FFS pattern in standard shoes.

107 Methods

108 *Participants*

Twenty nine participants, aged 18 - 60 years were included in the study (Table 1). These participants were part of a larger study of healthy runners. Participants were required to run at least 10 miles per week, with a minimum running pace of 8.5 minutes per mile (3.12 m.s⁻¹). Participants were injury-free at the time of data collection, and had been injury-free for at least six months prior. Habitual footwear was recorded. Foot strike was determined from frame-byframe observation of videos (125 frames per second) capturing force plate contact from a sagittal plane view. Only one camera was used, allowing observation of either the medial right foot, or

Accepted for publication in Medicine & Science in Sports & Exercise, June 2016

the lateral left foot. Foot strike pattern was observed from the video analysis for each trial, and 116 the participant was categorized as running with either a RFS (heel first landing) or a FFS 117 (forefoot first landing) based on observation of all of their recorded trials. No participants 118 119 demonstrated a combination of both RFS and FFS running in this study. Runners with a midfoot strike (flat foot landing), were not included in this study, as there were fewer than five midfoot 120 strike runners in each footwear condition. Once footstrike pattern was classified, those who ran 121 with a FFS pattern in traditional shoes and those who ran with a FFS pattern in minimal shoes 122 (defined as having minimal cushioning and heel-toe drop ≤ 4 mm) were included. An equal 123 number of those who run with a RFS pattern in traditional shoes were randomly selected and 124 were also included. The study was approved by the Institutional Review Board, and all 125 participants provided written informed consent. 126

127 *Protocol*

Each participant was provided with a shoe consistent with the type of shoe they habitually wore 128 for at least 50% of their running miles. The standard neutral lab shoe was the Nike Air Pegasus 129 and the minimal lab shoe was the inov-8TM BARE-X-200. Participants warmed up on a 130 treadmill, running at 2.24 m.s⁻¹ for three minutes, followed by overground running 131 familiarization trials. Force data were collected at 1500 Hz using two AMTI force plates (AMTI, 132 Watertown, MA). Data were collected while participants ran at 3.13 m.s⁻¹ (\pm 5%) along a 30 133 meter runway. Five trials per side in which the foot was completely on the force plate were 134 included. Participants were not aware that force data were being collected, or that foot strike was 135 being assessed, thus minimizing the likelihood of plate targeting or alteration of foot strike. 136

137 Data analysis

Accepted for publication in Medicine & Science in Sports & Exercise, June 2016

Force data were filtered using a 4th order 50Hz low-pass Butterworth filter in Visual3D (C-138 motion, Rockville, MD). Variables were extracted for each trial using customized Matlab 139 (Mathworks, Natick, MA) codes. Data from only those trials in which the right leg contacted the 140 force plate were used throughout. Stance was identified when vertical GRF > 10N. Variables 141 were obtained from each trial. Time series data were then time normalized and averaged across 142 trials for visualization purposes only. Comparisons were made between those who habitually run 143 with a RFS in a standard shoe (SRFS), those who habitually run with a FFS in a standard shoe 144 (SFFS), and those who habitually run with a FFS in a minimal shoe (MFFS). 145

146 Variables

Component ILRs were determined by calculating the derivative of the corresponding GRF with 147 respect to time. Resultant ILR was the resultant of component ILRs (rather than the derivative of 148 the resultant GRF). This ensured that positive ILR values were obtained, so that the resultant 149 magnitude would be more easily interpreted. GRF and ILR values were normalized to body 150 weight (BW). The percentage of foot strikes which included a vertical impact peak (VIP) was 151 determined for each group, where a VIP was defined as a local maximum in vertical GRF that 152 occurred prior to the overall maximum vertical GRF. These percentages were provided for 153 reference, and were not included in statistical analyses. Ground contact times were also 154 compared across groups. 155

Peak medial (negative direction) and lateral (positive direction) GRF values were obtained from the first 25% of stance. In the posterior (negative direction) GRF, an initial peak is often observed prior to the greatest peak value, particularly when FFS running. This posterior impact peak was defined as the greatest local minimum in the first 15% of stance. The maximum ILR

Accepted for publication in Medicine & Science in Sports & Exercise, June 2016

value in the first 25% of stance was obtained for the resultant, as well as in the vertical, lateral 160 and medial directions, while the posterior ILR was the maximum value in the first 15% of stance. 161 Previous studies of RFS running have obtained the vertical loadrate between 20% and 80% of 162 the time of the vertical GRF impact peak (6, 14, 17, 19, 21, 29, 32). However, when running with 163 a FFS pattern, an impact peak may not be present, in which case an alternative method is 164 required to calculate loadrate. Samaan et al. (26) utilized 13% of stance (the average time of an 165 impact peak in the RFS pattern) over which to calculate the loadrates in FFS runners. Boyer (2) 166 used a similar approach, but used 14% of stance. Goss (12) considered the loadrate for runners 167 without impact peaks between 3% and 12% of stance. As we have found vertical loadrate peaks 168 in FFS to occur later in the stance cycle, we calculated these over the first 25% of stance. 169 However, for comparison to other studies, we also calculated peak vertical loadrates in FFS 170 171 runners in the first 13% of stance (Peak vILR₁₃).

172 *Statistical analyses*

The data were determined to be non-normally distributed according to Kolmogorov-Smirnov 173 tests and the observation of histograms. Nonparametric Kruskal-Wallis tests were used to 174 identify whether there was a main effect of group on GRF and ILR variables, with P < 0.05175 indicating a significant main effect. Where there was a main effect, Mann Whitney U tests 176 identified where differences between groups occurred. A post-hoc sub-analysis was also 177 conducted on the minimal footwear group. This is because half of the shoes classified as minimal 178 had some cushioning (partial minimal, n=5) and half had no cushioning (full minimal, n=5). The 179 vertical and resultant ILR, as well as the percentage of foot strikes with impact peaks in these 180 two minimal footwear subgroups were compared descriptively to the two standard shoe groups. 181

182 **Results**

Demographic characteristics of the participants are presented in Table 1. There were 22 male and 7 female participants. The majority of those who habitually ran with a FFS in either footwear condition were male (89%). There were no differences in age, height, body mass or BMI between groups.

187 There was a main effect for ground contact time (P < 0.001), which was lowest in the SFFS group, and highest in the SRFS group [mean (SD) SRFS: 270 (23) ms; SFFS: 246 (20) ms; 188 189 MFFS: 260 (10) ms, P < 0.001 for all comparisons]. Impact peaks, defined as local maxima 190 during early stance, were present in 96% of foot strikes in the SRFS group, compared with 16% 191 in the SFFS group and 32% in the MFFS group. Group mean GRF and ILR time histories are 192 presented in Figures 1 (resultant and vertical) and 2 (AP and ML directions). Peak GRF and ILR values are presented in Figures 3 and 4 respectively. There were main effects for posterior, 193 lateral, and medial impact peaks (P < 0.001 in all cases). Posterior impact peak was lowest in the 194 195 SRFS group, and highest in the SFFS group. Lateral impact peak was lower in the MFFS group than both standard shoe groups. Medial impact peak was higher in the SFFS group than both the 196 SRFS and MFFS groups. 197

There were main effects for ILR in all directions, including the resultant (P < 0.001 in all cases). Resultant and vertical ILR were lower in MFFS than both standard shoe groups. Posterior ILR values were higher in the SFFS group than both the SRFS and MFFS groups. Lateral and medial ILR values were lower in MFFS than both standard shoe groups. Peak vertical ILR calculated over the first 13% of stance (Peak vILR₁₃) was higher in the SRFS group than both the SFFS (P = 0.007) and MFFS (P < 0.001) groups [mean (SD) SRFS: 71.12 (27.70) BW.s⁻¹; SFFS: 55.24

Accepted for publication in Medicine & Science in Sports & Exercise, June 2016 (14.22) BW.s⁻¹; MFFS: 47.10 (12.00) BW.s⁻¹]. Time of peak vertical ILR (mean (SD) values as a percentage of stance) occurred at 9.0 (2.2) % in SRFS; 14.4 (4.2) % in SFFS; and 10.6 (7.5) % in MFFS runners. The range of values for time of peak vertical ILR for the SRFS, SFFS and MFFS groups respectively were 4.4 - 12.7 %; 5.0 - 20.3 %; and 1.7 - 24.5 %.

208

209 Sub-analysis results

Both partial and full minimal shoe subgroups exhibited lower resultant and vertical loadrates than the groups who either RFS or FFS in standard shoes. However, vertical and resultant ILR were 17% and 15% lower respectively in those who habitually FFS in *full* minimal shoes compared with those who habitually FFS in *partial* minimal shoes (Figure 5). Additionally, all of the impact peaks noted in the minimally shod group (32% of footstrikes) were found in those who habitually run in partial minimal shoes. Those habituated to full minimal shoes exhibited no impact peaks.

217

218 **Discussion**

The purpose of this study was to determine the influence of foot strike and footwear on component and resultant ground reaction forces and loadrates in runners in their habitual conditions. Results of this study suggest that forefoot striking in shoes with the least cushioning results in the lowest rates of loading.

223 Ground Reaction Force

Accepted for publication in Medicine & Science in Sports & Exercise, June 2016

GRF time histories displayed patterns that differed according to foot strike pattern. When 224 running with a RFS, the majority of foot strikes displayed a distinct impact peak, which was not 225 the case when running with a FFS in either shoe. This is consistent with previous findings (12, 226 227 13). Distinct posterior and medial impact peaks were observed in both FFS groups which were less evident when running with a RFS, also consistent with previous findings (2, 3, 18, 29). 228 Boyer et al., (2) suggested that the initial posterior and medial impact peaks that occur during 229 FFS running may result from a rapid change in direction of the foot center of mass during stance, 230 which does not occur during RFS running. The lower lateral GRF when running in minimal 231 shoes compared with standard shoes may be the result of a smaller lateral flare in minimal shoes 232 than standard shoes. This results in a smaller moment arm for the vertical ground reaction force, 233 thereby reducing the pronatory moment on the foot. This may minimize the amount of change in 234 235 direction of the center of pressure at contact. The mechanical characteristics of the shoe, particularly the rigidity, likely also influence the amount of change in direction of the center of 236 pressure throughout stance. The magnitude of GRF in the AP and ML directions is considerably 237 238 lower than in the vertical direction for all groups. Nonetheless, these components contribute to the shear forces applied to the body and may be important in terms of injury. For example it is 239 known that bone is weaker in shear than compression (28). 240

241 Instantaneous loadrates

Our results were consistent with a previous study, demonstrating similar resultant ILR between habitual RFS and FFS runners in traditional footwear (2). In their study, Boyer et al. (2) found a significantly lower vertical ILR in FFS runners, but the resultant was similar due to higher posterior and medial ILR. In our study, the component ILR values were similar between foot strikes when running in standard running footwear, with non-significantly lower vertical ILR but

Accepted for publication in Medicine & Science in Sports & Exercise, June 2016

higher posterior ILR contributing to a similar resultant ILR. In the current study, runners who 247 habitually use minimal shoes and run with a FFS had lower component and resultant loadrates 248 than runners using standard footwear with either foot strike. This finding is likely due to an 249 250 interaction of footstrike pattern and footwear, as running with a RFS pattern in minimal shoes results in higher loadrates than in standard shoes (20). Those who habitually run in *full* minimal 251 shoes had lower vertical and resultant loadrates than those who habitually run in *partial* minimal 252 shoes. Additionally, only those running in partial minimal shoes exhibited impact peaks in their 253 vertical ground reaction forces. This further emphasizes the importance of footwear, and 254 suggests that even being habituated to a small amount of cushioning can lead to harder landings. 255 To date, only the vertical ILR component has been associated with injury in runners. However, 256 the resultant warrants investigation as these loadrates are at least as high as the vertical ILR, and 257 258 represent the total loading experienced by the body.

259 When running with a FFS, the foot contacts the ground in a more plantarflexed (30) and inverted (2) position than when running with a RFS. To achieve a FFS in standard shoes, these 260 characteristics may be exaggerated in order to overcome both the heel height and lateral flare of 261 the standard shoe, that are not present in a true minimal shoe. This may increase both the braking 262 and mediolateral forces in early stance, and could lead to higher loadrates. Furthermore, the 263 midsole of a standard shoe extends to the forefoot and provides additional cushioning. Several 264 studies have demonstrated that individuals land harder when landing on cushioned surfaces (1, 265 10, 16). 266

While the vertical loadrate was lower in the SFFS compared with the SRFS, this was not statistically different, contrary to our hypothesis and to previous studies (2). The current study identified the maximum loadrate within the first 25% of stance, while previous studies used only

Accepted for publication in Medicine & Science in Sports & Exercise, June 2016

the first 13% of stance (4, 6, 13, 17, 19, 21, 26, 29). When assessing vertical loadrates within the first 13% of stance, our findings also indicated significantly lower vertical ILR when running with a FFS compared with a RFS. However, our findings demonstrate that the time of peak vertical ILR ranged from 1.7% to 24.5% of stance when running with a FFS, thus the maximum vertical loadrate may not have been obtained in previous studies including FFS runners.

Vertical ILR for FFS runners in both shoe conditions demonstrated two local maxima, with the 275 first local maximum being lower than the second. Boyer et al. (2) also found a double peaked 276 vertical ILR for the FFS group, however, they found the second peak to be lower than the first. 277 The source of this second peak may be associated with the acceleration of the remainder of the 278 body's mass throughout stance, following initial foot contact (5). The difference observed 279 between the present study, and the study by Boyer et al. may be due to the combining of MFS 280 and FFS data in the previous study, while our study included only FFS runners. Furthermore, the 281 282 study by Boyer et al. included competitive runners, whereas our study included recreational runners. Both of these factors likely influenced the acceleration of the remainder of the body's 283 mass after foot impact. All other studies of FFS running, because of the range over which they 284 assessed loadrates, captured the first peak in vertical ILR, but not the second. Therefore, they 285 may have underestimated the true vertical instantaneous loadrate during the loading phase of 286 stance. Future studies of FFS running should consider the maximum vertical ILR that occurs 287 throughout the first 25% of stance, rather than determining this according to the typical time of 288 impact peak when running with a RFS pattern. 289

This study has a number of strengths. First, including runners in their habitual running conditions increases the ecological validity of the results. Additionally, including an assessment of resultant ILR provides information about the total loading experienced by the body. Finally,

Accepted for publication in Medicine & Science in Sports & Exercise, June 2016

extending the range of stance over which instantaneous loadrates are assessed in FFS runners improves the validity of the data. This study may have been limited by the uneven distribution of gender between the groups, although there is no evidence that this factor affects impact loading. This observed difference may be interesting in itself, and warrants further investigation. Additionally, while habitually running with a FFS pattern in a minimal shoe resulted in lower loadrates than in a standard shoe, further studies are required to determine if these differences are important in terms of injury.

300

301 Conclusions

The results of this study suggest that running with a FFS pattern in standard shoes results in similar resultant loadrates as running with a RFS pattern in standard shoes. However, resultant loadrates are significantly lower when running with a FFS pattern in minimal shoes. Preliminary analysis of the minimal footwear group revealed that runners who are habituated to full minimal shoes (no cushioning) have the lowest impacts at landing. Additional studies are under way to further examine these differences.

308

309 Acknowledgements

The authors would like to acknowledge the contributions of those who assisted with this project at the Spaulding National Running Center, including Matt Ruder, Phattarapon Atimetin, and Erin Futrell. The results of this study do not constitute endorsement by ACSM. There are no funding sources to disclose for this work. Rice, Jamison & Davis Accepted for publication in Medicine & Science in Sports & Exercise, June 2016

314

315 **Conflict of Interest**

316 We report no known conflicts of interest.

317 **References**

- Bishop M, Fiolkowski P, Conrad B, Brunt D, Horodyski M. Athletic footwear, leg stiffness, and running kinematics. *J Athl Train* 2006;41(4):387.
- Boyer ER, Rooney BD, Derrick TR. Rearfoot and midfoot or forefoot impacts in habitually
 shod runners. *Med Sci Sports Exerc* 2014;46(7):1384–1391.
- Cavanagh PR, Lafortune MA. Ground reaction forces in distance running. *J Biomech* 1980;13(5):397–406.
- Cheung R, Davis I. Landing Pattern Modification to Improve Patellofemoral Pain in Runners: A Case Series. *J Orthop Sports Phys Ther* 2011;41(12):914–9.
- 5. Clark KP, Ryan LJ, Weyand PG. Foot speed, foot-strike and footwear: linking gait
 mechanics and running ground reaction forces. *J Exp Biol* 2014;jeb.099523.
- 328 6. Crowell HP, Davis IS. Gait retraining to reduce lower extremity loading in runners. *Clin Biomech* 2011;26(1):78–83.
- 330 7. Daoud AI, Geissler GJ, Wang F, Saretsky J, Daoud YA, Lieberman DE. Foot strike and
 injury rates in endurance runners: a retrospective study. *Med Sci Sports Exerc*332 2012;44(7):1325–34.
- Bavis IS, Bowser BJ, Mullineaux DR. Reduced vertical impact loading in female runners
 with medically diagnosed injuries: a prospective investigation. *Br J Sports Med* 2015;bjsports-2015-094579.
- 336 9. Diebal AR, Gregory R, Alitz C, Gerber JP. Forefoot running improves pain and disability
 337 associated with chronic exertional compartment syndrome. *Am J Sports Med*338 2012;40(5):1060–7.
- Ferris DP, Farley CT. Interaction of leg stiffness and surfaces stiffness during human
 hopping. *J Appl Physiol Bethesda Md 1985* 1997;82(1):15-22-14.
- Giuliani J, Masini B, Alitz C, Owens BD. Barefoot-simulating Footwear Associated With
 Metatarsal Stress Injury in 2 Runners [Internet]. *Orthopedics* 2011; [cited 2015 Jan 29]
 Available from: http://www.slackinc.com/doi/resolver.asp?doi=10.3928/0147744720110526-25

Accepted for publication in Medicine & Science in Sports & Exercise, June 2016

- Goss DL, Gross MT. A comparison of negative joint work and vertical ground reaction
 force loading rates in Chi runners and rearfoot-striking runners. *J Orthop Sports Phys Ther* 2013;43(10):685–692.
- Kulmala J-P, Avela J, Pasanen K, Parkkari J. Forefoot strikers exhibit lower runninginduced knee loading than rearfoot strikers. *Med Sci Sports Exerc* 2013;45(12):2306–13.
- Laughton CA, Davis IM, Hamill J. Effect of strike pattern and orthotic intervention on
 tibial shock during running. *J Appl Biomech* 2003;19(2):153–168.
- 15. Lieberman DE, Venkadesan M, Werbel WA, et al. Foot strike patterns and collision forces
 in habitually barefoot versus shod runners. *Nature* 2010;463(7280):531–5.
- McNitt-Gray JL, Yokoi T, Millward C. Landing Strategies Used by Gymnasts on Different
 Surfaces. *J Appl Biomech* 1994;10(3):237–52.
- Milner CE, Ferber R, Pollard CD, Hamill J, Davis IS. Biomechanical factors associated
 with tibial stress fracture in female runners. *Med Sci Sports Exerc* 2006;38(2):323–8.
- 18. Nilsson J, Thorstensson A. Ground reaction forces at different speeds of human walking
 and running. *Acta Physiol Scand* 1989;136(2):217–27.
- Noehren B, Scholz J, Davis I. The effect of real-time gait retraining on hip kinematics, pain
 and function in subjects with patellofemoral pain syndrome. *Br J Sports Med* 2011;45(9):691–6.
- Paquette MR, Zhang S, Baumgartner LD. Acute effects of barefoot, minimal shoes and
 running shoes on lower limb mechanics in rear and forefoot strike runners. *Footwear Sci*2013;5(1):9–18.
- Pohl MB, Hamill J, Davis IS. Biomechanical and Anatomic Factors Associated with a
 History of Plantar Fasciitis in Female Runners: *Clin J Sport Med* 2009;19(5):372–6.
- Radin EL, Parker HG, Pugh JW, Steinberg RS, Paul IL, Rose RM. Response of joints to
 impact loading III. *J Biomech* 1973;6(1):IN9-IN11.
- Radin EL, Paul IL. Response of joints to impact loading. I. In vitro wear. *Arthritis Rheum*1971;14(3):356–62.
- Ridge ST, Johnson AW, Mitchell UH, et al. Foot bone marrow edema after a 10-wk
 transition to minimalist running shoes. *Med Sci Sports Exerc* 2013;45(7):1363–8.
- Salzler MJ, Bluman EM, Noonan S, Chiodo CP, Asla RJ de. Injuries Observed in
 Minimalist Runners. *Foot Ankle Int* 2012;33(4):262–6.
- Samaan CD, Rainbow MJ, Davis IS. Reduction in ground reaction force variables with
 instructed barefoot running. *J Sport Health Sci* 2014;3(2):143–51.

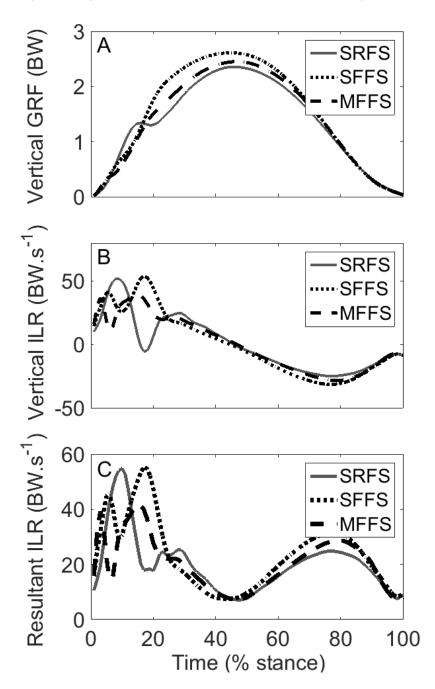
Accepted for publication in Medicine & Science in Sports & Exercise, June 2016

378 379 380	27.	Squadrone R, Gallozzi C. Biomechanical and physiological comparison of barefoot and two shod conditions in experienced barefoot runners. <i>J Sports Med Phys Fitness</i> 2009;49(1):6–13.	
381 382	28.	Turner CH, Wang T, Burr DB. Shear strength and fatigue properties of human cortical bon determined from pure shear tests. <i>Calcif Tissue Int</i> 2001;69(6):373–8.	
383 384	29.	Williams DS, McClay IS, Manal KT. Lower Extremity Mechanics in Runners with a Converted Forefoot Strike Pattern. <i>J Appl Biomech</i> 2000;16(2):210–8.	
385 386 387	30.	Williams DSB, Green DH, Wurzinger B. Changes in lower extremity movement and power absorption during forefoot striking and barefoot running. <i>Int J Sports Phys Ther</i> 2012;7(5):525–32.	
388 389	31.	Zadpoor AA, Nikooyan AA. The relationship between lower-extremity stress fractures and the ground reaction force: A systematic review. <i>Clin Biomech</i> 2011;26(1):23–8.	
390 391	32.	Zifchock RA, Davis I, Hamill J. Kinetic asymmetry in female runners with and without retrospective tibial stress fractures. <i>J Biomech</i> 2006;39(15):2792–7.	
392			
393			

Main Effect Variable SRFS (n=10) SFFS (n=9) MFFS (n=10) **(P)** Male: Female 5:5 7:2 10:0 Age (years) 32.2 (9.1) 30.7 (10.0) 41.0 (10.9) >0.05 1.72 (0.11) Height (m) 1.76 (0.08) 1.82 (0.05) >0.05 Body mass (kg) 69.3 (15.6) 70.3 (7.3) 78.0 (13.1) >0.05 BMI $(m.kg^{-2})$ 23.2 (3.7) 22.7 (1.7) 23.6 (2.9) >0.05

394Table 1: Mean (SD) demographics for each group

395

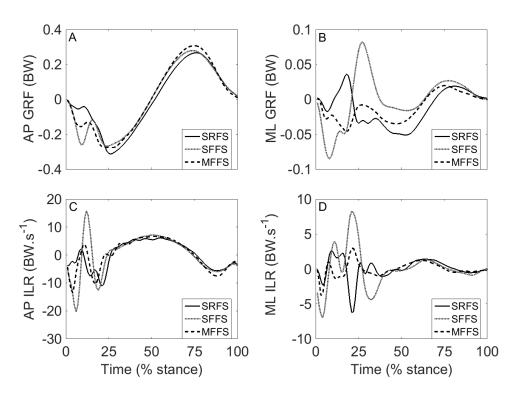


397

Figure 1: Group mean vertical GRF (A), vertical ILR (B) and resultant ILR (B) throughoutstance.

400

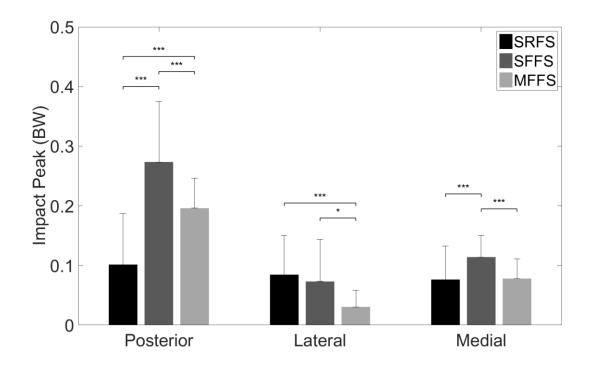
Rice, Jamison & Davis Accepted for publication in Medicine & Science in Sports & Exercise, June 2016



402

Figure 2: Group mean GRF (A and B) and ILR (C and D) throughout stance in the AP (A and C)
and ML (B and D) directions. Positive values represent lateral and anterior directions,
respectively.

Rice, Jamison & Davis Accepted for publication in Medicine & Science in Sports & Exercise, June 2016



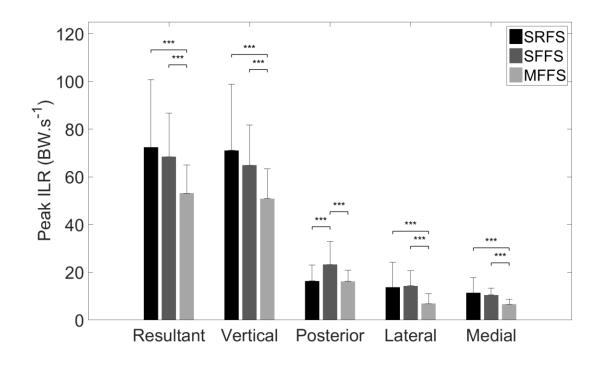
407

408 Figure 3: Group mean (SD) GRF impact peaks in the posterior, lateral and medial directions.

409 ^{*} indicates significant difference between groups, P < 0.05

410 ^{****} indicates significant difference between groups, P < 0.001

Rice, Jamison & Davis Accepted for publication in Medicine & Science in Sports & Exercise, June 2016



413 Figure 4: Group mean (SD) values for resultant and component peak ILR.

414	*** indicates significant d	lifference between	groups, $P < 0.001$
	\mathcal{O}		

415

Rice, Jamison & Davis Accepted for publication in Medicine & Science in Sports & Exercise, June 2016

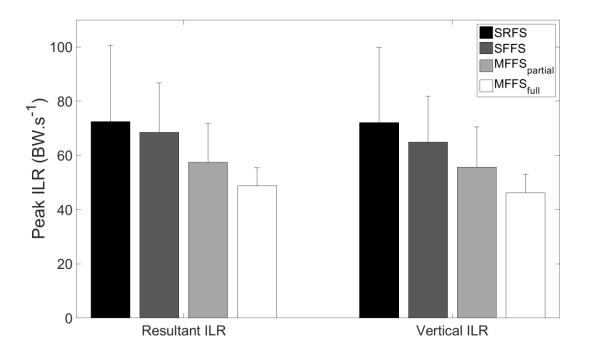


Figure 5: Group mean (SD) peak resultant ILR and vertical ILR values. MFFS subgroup values
are presented, where MFFS_{partial} represents those who habitually run in partial minimal shoes,
and MFFS_{full} represents those who habitually run in full minimal shoes.