

1 **QUANTIFYING BI-VARIATE COORDINATION VARIABILITY DURING LONGITUDINAL MOTOR**
2 **LEARNING OF A COMPLEX SKILL**

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10
11 **Abstract:** Biofeedback (BFb) can enhance the motor learning process by
12 guiding skill exploration. Too much BFb, however, can foster dependency
13 leading to skill retention deficits once removed. A reducing BFb schedule
14 could negate dependency effects, however limited methodologies exist to
15 assess the effectiveness of an intervention during application. This research
16 proposes a new bi-variate method ($CI2_{Area}$) to quantify coordination
17 variability ($Coord_{Var}$) as a measure of skill exploration during a motor learning
18 intervention. Thirty-two participants were introduced to a novel explosive-
19 lunge task. A BFb group ($n=16$) were provided with visual BFb on rear hip,
20 knee and ankle joint extension magnitudes and timing during a 26-week
21 reducing schedule BFb intervention. $Coord_{Var}$ of hip-knee and knee-ankle
22 angular velocities were quantified by calculating the area encompassed by
23 the 95% confidence intervals of joint coupling angular-velocity bi-variate
24 plots ($CI2_{Area}$). Linear regressions were fitted to group and individual $Coord_{Var}$
25 longitudinal data. The BFb was effective in successfully altering whole limb
26 technique within just two sessions, and these changes were retained. The
27 BFb group demonstrated a continual increase of $Coord_{Var}$ throughout the
28 intervention, showing continual skill exploration strategies, while the
29 Control group remained unchanged. Gradually increasing time between
30 sessions, using a longitudinally reducing BFb schedule, successfully negates
31 dependency effects on BFb while also encouraging motor learning.
32 Manipulating time between sessions allows for the provision of a high
33 frequency of 100% BFb without fostering dependency. The $CI2_{Area}$ method
34 was able to detect individual exploration strategies and could be used in the
35 future to direct individual intervention modifications.

36 **KEYWORDS:** BIOFEEDBACK, KNOWLEDGE OF PERFORMANCE, BIOMECHANICS

38 **1. Introduction**

39 Biofeedback (BFb) is an effective tool to facilitate and accelerate the skill development
40 process (Swinnen et al., 1997; Baudry et al., 2006; Thow et al., 2012; Baggaleley et al., 2017).
41 The provision of information relating to movement parameters, termed knowledge of
42 performance or KP, has proven to be effective in developing specific movement patterns
43 (Ford et al., 2015). In contrast, the constrained action hypothesis considers that feedback
44 directed on specific movement restricts explorative strategies, and instead focus should be
45 directed to information sources outside of the body (Wulf and Shea, 2002). Much of the
46 constrained action hypothesis research is based on a focus of attention using instruction (i.e.
47 how to achieve a movement pattern) rather than feedback (i.e. how a skill was executed). In
48 comparing the focus of attention, feedback has been shown to be more effective than both
49 internal and external instruction in targeting specific movement patterns (Keller et al., 2014).
50 Short term BFb interventions applied to improve sporting performance (Broker et al., 1993;
51 Eriksson et al., 2011), reduce injury risk (Crowell et al., 2010; Ford et al., 2015; Creaby and
52 Smith, 2016) and in clinical rehabilitation (van den Heuvel et al., 2016) have shown changes
53 to occur within just a few visits, but there is limited information on how influential or
54 permanent these changes are. Longer, higher frequency BFb schedules, such as eight sessions
55 during a four-week period (Mullineaux et al., 2012) and 36 sessions in 12 weeks (Viitasalo et
56 al., 2001) have shown more permanent modifications.

57 Long and high frequency interventions are, however, time and resource intensive. From a
58 theoretical perspective, the guidance hypothesis considers that while BFb is beneficial to
59 direct motor learning, too much BFb can lead to dependency and prevent autonomous
60 exploration processes (Salmoni et al., 1984; Sadowski et al., 2013). This dependency may

61 encourage learners to bypass other important sources of feedback information needed to
62 develop intrinsic error detection and correction mechanisms (Park et al., 2000). To reduce any
63 dependency, BFb frequency over time can be reduced (e.g. Richards et al., 2018b) and time
64 between visits can be increased. BFb dependency is typically evidenced with a drop-off in
65 retention once BFb is removed (Maslovat et al., 2009), and is considered to be skill specific
66 (Sigrist et al., 2013; Wulf and Shea, 2002). No methods have currently been used, however,
67 to assess skill exploration during the intervention period, and such a method may be
68 beneficial in identifying dependency or identifying occurrences of skill exploration.

69 Movement variability, comprising of functional and non-functional components (Cazzola et
70 al., 2016; Hamill et al., 1999; Preatoni et al., 2013), can provide a measure of skill exploration.
71 From a dynamical systems perspective, coordination variability ($Coord_{var}$) is functional to
72 allow the motor system to adapt to perturbations within the task, individual or environment
73 (Bernstein, 1967) to facilitate consistent skill outcome (Mullineaux and Uhl, 2010; Robins et
74 al., 2006). Consistency of skill outcome, or performance variability ($Perf_{var}$), in contrast is often
75 considered non-functional in influencing skill execution. An integral component of motor
76 learning paradigms is the notion of freezing and freeing degrees of freedom with skill
77 development during stages of motor learning within and between individuals (e.g. Berstein,
78 1967; Newell, 1985). $Coord_{var}$, as an analytical tool, has been used to identify subtle
79 differences in skill execution between novice, skilled and elite performance (Cazzola et al.,
80 2016), and has been more sensitive when conventional biomechanical approaches have failed
81 to distinguish between patients with subtle pathologies (Hamill et al., 1999). $Coord_{var}$ may
82 therefore provide a specific tool to assess skill exploration during an intervention, thus also

83 allowing individual analyses in line with some biomechanical paradigms to assess the
84 individual instead of the group (Glazier and Mehdizadeh, 2018; Needham et al., 2018).

85 Methods to quantify $\text{Coord}_{\text{Var}}$ require careful consideration. Vector coding (VC) is a widely
86 used measure of coordination between two joints or segments (e.g. Hamill et al., 1999;
87 Needham, 2014; 2015). The standard deviation of the vector angle (Heiderscheit et al., 2002)
88 or standard deviation of both the vector angle and length (Tepavac and Field-Fote, 2002)
89 provide a measure of $\text{Coord}_{\text{Var}}$, but both VC methods are susceptible to noise artefacts related
90 to changes in vector length that can overinflate the variability output (Stock et al., 2018). An
91 alternative bi-variate data analysis method, CI2, allows for the real-world coordination of any
92 two time series data sets to be compared (Mullineaux, 2017). The first stage of this approach
93 applies ellipses to encompass multiple trials of the bivariate data at each time point, with the
94 ellipse axes scaled to 95% confidence intervals (95%CI). Stock et al. (2018) used these 95%CI
95 ellipses to encase multiple trial angle-angle vector end points, identifying the area of these
96 ellipses to be more robust to the statistical artefacts found using VC. CI2 uses quadrilaterals
97 to connect consecutive ellipses to create 95%CI boundaries for the entire time series. The CI2
98 Matlab code provided by Mullineaux (2017) can be modified to extract the area of these
99 quadrilaterals (CI2_{Area}) to provide a measure to statistically compare the spread, or $\text{Coord}_{\text{Var}}$,
100 between any bi-variate time series.

101 Therefore, the aims of this research were to: 1) identify when changes occurred in targeted
102 Bfb variables during a 6-month longitudinal Bfb intervention of a complex skill, and; 2) apply
103 a new measure of coordination variability, CI2_{Area} , to assess skill exploration as a measure of
104 Bfb effectiveness or dependency during the intervention.

105

106 **2. Methods**

107 *2.1 Participants*

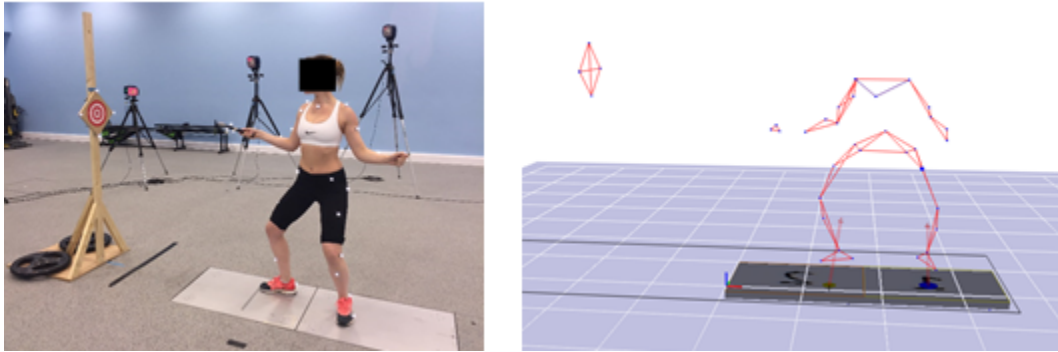
108 Following institutional ethical approval, thirty-two healthy participants were recruited who
109 were physically active, injury free, aged 18-40 years old and provided informed consent.
110 Individuals were also screened for green-red colour blindness. Participants were randomly
111 assigned into either BFb (n=16; 7 male, 9 female; means \pm SD; age 26 ± 5 years, height $1.71 \pm$
112 0.06 m, mass 67.4 ± 10.76 kg, leg length 0.91 ± 0.04 m) or Control groups (n=16; 8 male, 8
113 female; age 24 ± 4 years, height 1.72 ± 0.10 m, mass 70.1 ± 14.9 kg, leg length 0.92 ± 0.06 m).

114

115 *2.2 Procedure*

116 Participants visited the laboratory on six occasions over a six-month period structured as a
117 longitudinally reducing schedule, meaning an increase in duration between each visit (i.e.
118 from 24 hours increasing up to 12 weeks between visits). During the first week participants
119 attended three sessions, spaced 24-48 hours apart. During visit one, all participants
120 undertook three blocks (6 lunges/block) of 'self-learning' following instruction on a novel
121 lunge touch task to propel themselves forward as quickly as possible and use a 20 cm long
122 pointer to strike a 15 x 15 cm target placed 1.5 leg lengths away from the front foot (figure
123 1). Each foot was on an individual force plate, with the front foot pointed toward the target
124 and the rear foot perpendicular to the target. Elbows were tucked in, with participants
125 crouching to 130° of flexion at the rear knee.

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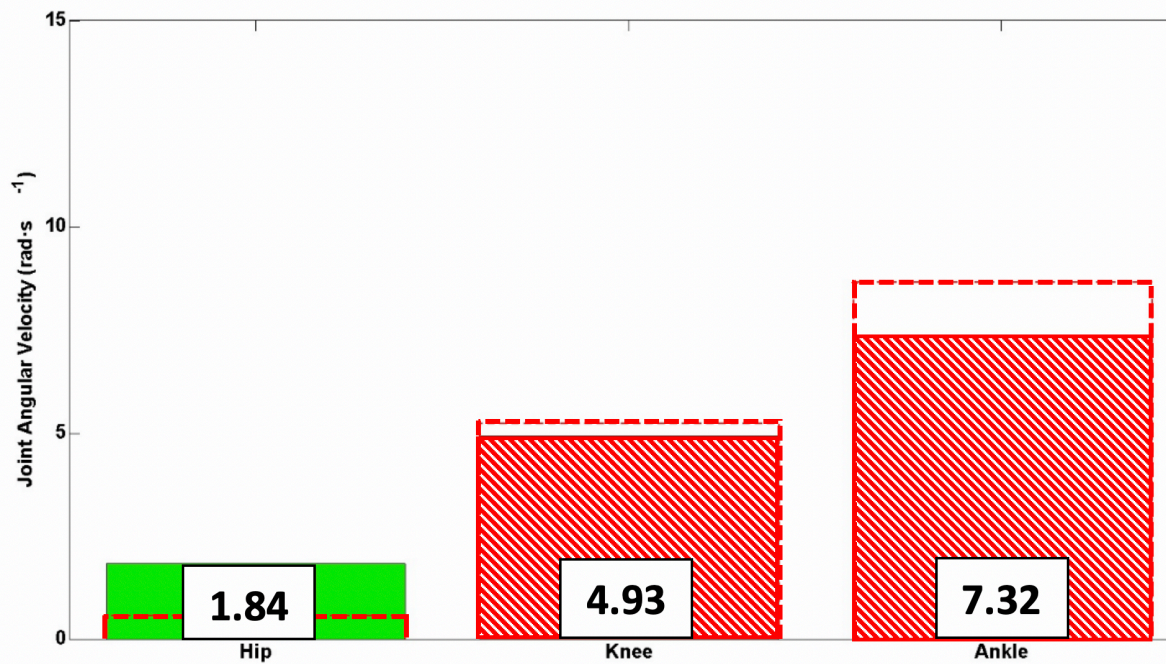


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128 **Figure 1.** Photograph (left) and motion capture software screenshot (right) of a participant in
129 the start pose, and illustrating the marker set up, target and force plate position.

130

131 The task was based on the explosive element of an attacking lunge in fencing. A measure of
132 task success was maximal horizontal centre of mass (CoM) propulsion as linked to lunge
133 success in fencing (Yiou and Do, 2000; Bottoms et al., 2013). Following the self-learning, the
134 BFb group were provided with instruction on BFb. Within 10s of each lunge each BFb
135 participant received BFb on the magnitude and timing of rear leg hip, knee and ankle maximal
136 angular extension velocities. The BFb was displayed as a bar-chart with a colour coding system
137 used to demonstrate sequencing information using joint angular velocity timing (green-
138 signifying proximo-distal sequencing; red identifying joints that were out of sequence; figure
139 2). Participants were instructed to obtain proximo-distal sequencing, which has been linked
140 with successful fencing attacking lunge performance (Mulloy et al., 2018), while also trying to
141 beat their personal best maximal joint angular velocities that was displayed as an overlaid red
142 dotted line for each joint. The personal best trial was the trial with the greatest ankle plantar-
143 flexion maximal velocity during that session.



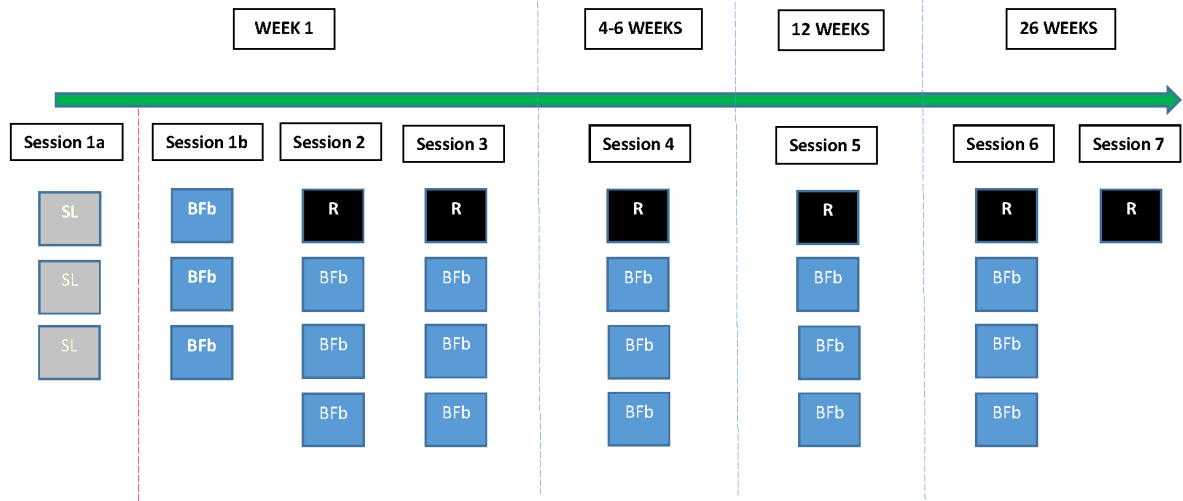
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145 **Figure 2.** Biofeedback presentation on the magnitude and timing of rear leg hip, knee and
 146 ankle maximal angular extension velocity. The red-dotted line represents the session personal
 147 best trial for all three joints. Colour coding was used to display joint sequencing information,
 148 with patterns added here for visual clarity. All green (no pattern) signified proximal to distal
 149 sequencing, and red (striped pattern) identifying joints that were out of sequence (knee and
 150 ankle in this example). Values indicate joint angular velocity for the last trial completed.

151

152 All subsequent sessions comprised of one block of retention lunges (no BFb) followed by three
 153 blocks of BFb throughout the intervention. Following the intervention week, participants
 154 returned at 4-6 weeks (blocks 15-18) and 13 weeks (blocks 19-22), and then for a final
 155 retention session at 26 weeks (block 23; figure 3). The Control group matched all lunges but
 156 received no BFb throughout.

157



158

159 **Figure 3.** Schematic representation of longitudinal data collection protocol. Each square
 160 represents 1 block. SL = self-learning, where no BFb was provided; BFb = 100% BFb (or no BFb
 161 for Controls) and R = a retention block. The order of blocks are referred to in the text from 1
 162 to 23. Blocks are separated by 2-3 minutes within a session, and sessions are on different days.

163

164 2.3. Data Analysis

165 Kinematic data were collected using 12 Raptor cameras sampling at 150 Hz with Cortex v5.3
 166 software (Motion Analysis Corporation, Santa Rosa, CA). Kinetic data were sampled at 1500
 167 Hz through two piezoelectric force plates (9281E, Kistler, Switzerland). Thirty 12.5 mm retro
 168 reflective markers were placed on lateral anatomical landmarks of the whole body, with four
 169 additional markers placed on the target, and three on the hand-held pointer. Custom written
 170 Matlab code (R2015a, Mathworks, Natick, MA) was used to analyse each trial. All data were
 171 smoothed using a zero lag, fourth-order, Butterworth low-pass filter with cut off frequencies
 172 of 10Hz for kinematic and 50Hz for kinetic data. Kinetic data from the rear foot force plate
 173 were used to identify key events to extract BFb data for presentation. Two key events were
 174 defined; onset of force (F_0) and take off (F_{TO}). F_0 was identified as the first frame that the rear

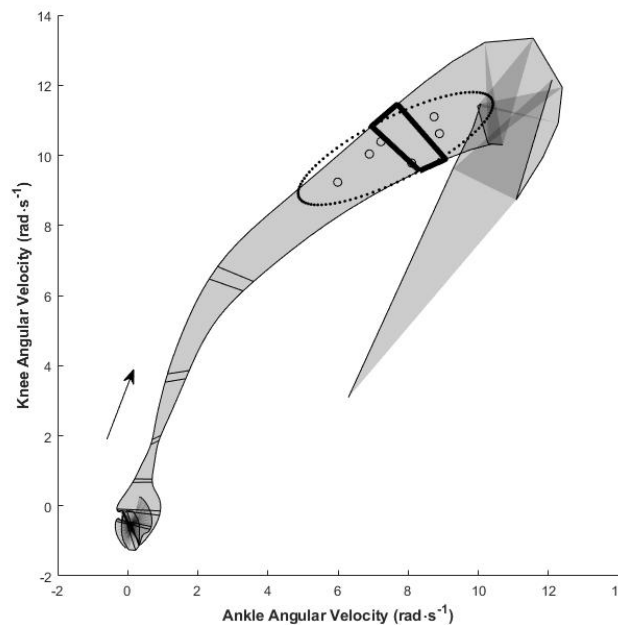
175 leg resultant force was exceeded and remained greater than 10% body weight from the
176 combined front and rear leg force plates. A robust F_{TO} time event was identified as the point
177 that the differentiated rear leg resultant force data crossed zero following peak force. Push
178 off ($F_{PushOff}$) was the phase defined from F_O to F_{TO} . Throughout $F_{PushOff}$ three-dimensional (3D)
179 vector angles were calculated for the rear leg hip, knee and ankle using thigh, shank and ankle
180 segments. The thigh segment was defined between the greater trochanter (GT) to the lateral
181 femoral condyle markers, the shank segment from the lateral femoral condyle to the lateral
182 malleolus markers, and the foot segment from the lateral malleolus to the fifth metatarsal
183 markers. The hip joint angle was defined as the angle between the thigh segment relative to
184 the forward horizontal, the knee joint angle between the thigh to the shank segments, and
185 the ankle joint angle between the shank to the foot segments. Local maxima joint extension
186 velocities were identified for the three rear leg joints and were presented as a percentage
187 change relative to the final block of 'self-learning' lunges (i.e. block 3 = 0%).

188

189 *2.4. Coordination Variability Calculation*

190 Hip, knee, and ankle joint velocity time series data were used to assess $Coord_{Var}$. Angular
191 velocities were selected for analysis as the primary variable targeted by the Bfb. Due to two
192 missing blocks of data, one Bfb participant was removed from the $Coord_{Var}$ analysis. Hip-knee
193 and knee-angle joint couplings $Coord_{Var}$ were quantified using a modification of a bivariate
194 analysis method (CI2, Mullineaux, 2017) to extract the CI2 area ($CI2_{Area}$). The first three stages
195 of CI2 were from code provided by Mullineaux (2017) to: 1) calculate 95%CI ellipses around
196 the cluster of joint coupling angular velocity data points for each frame; 2) join the centres of
197 consecutive ellipses to define the direction vector, and; 3) create convex quadrilaterals to

198 provide 95%CI borders along the entire time series (described in more detail in figure 4).
 199 $CI2_{Area}$ extracts the area encompassed by these quadrilaterals throughout $Push_{Off}$ calculated
 200 using the Matlab function 'polyarea'. A larger $CI2_{Area}$ was considered to demonstrate a greater
 201 exploration of the joint angular velocity coupling. $CI2_{Area}$ provided a discrete value for each
 202 block, for each participant, for the entire 26-week intervention as a measure of $Coord_{Var}$.



203

204 **Figure 4.** Example of $CI2_{Area}$ applied to the knee-ankle angular velocity joint coupling. The
 205 quadrilaterals at every 10% time points are illustrated for 6 trials, with the ellipse and raw
 206 data (data points) at 80% included for visual purposes. The 95% confidence ellipses encompass
 207 the data points at each time point throughout the data series, with the ellipse centres joined
 208 to create the direction vector. The points of the ellipse border perpendicular to the direction
 209 vector for two consecutive ellipses are then used to create quadrilaterals for the whole time
 210 series, with the area of the quadrilaterals being summed to provide $CI2_{Area}$.

211

212 2.5. Statistical Analysis

213 *Kinematic Changes*

214 Piecewise linear regressions were used to determine the session in which a change in
215 learning, or session breakpoint (S_{BP}), occurred for the local maxima joint extension velocities.
216 This process allowed for an identification of where improvements in skill plateaued during
217 the BFb schedule over the 26 weeks. Single outliers were removed using a median
218 anomaly detection method (Mullineaux and Irwin, 2017). Following confirmation of a normal
219 distribution (Shapiro-Wilk test > 0.05), an independent t-test was used to confirm that the
220 BFb had improved targeted kinematic variables more than the Control group at the S_{BP} for
221 hip, knee and ankle peak angular velocity percentage changes. Peak angular velocity changes
222 at retention time points for each joint were analysed using mixed ANOVAs (2 group x 3 times
223 of Retention_{Wk4-6}, Retention_{Wk13} Retention_{Wk26}). Where 95%CI were greater than zero would
224 be considered to indicate learning had occurred, and in combination with no significant
225 interactions would indicate that learning was relatively permanent. Descriptive statistics were
226 presented as means \pm 95%CI, and alpha was set at 0.05.

227

228 *Changes in Coordination Variability*

229 To determine changes in $Coord_{Var}$ across the 26 weeks, simple linear regressions were fitted
230 to the CI_{2Area} means for both groups and both joint couplings. The $Coord_{Var}$ gradients
231 ($CV_{Gradient}$) and 95%CI of the gradients ($95\%CI_{Gradient}$) of these regressions were calculated, and
232 where the BFb group's $CV_{Gradient}$ was greater than the Control group's $95\%CI_{Gradient}$ indicated
233 that the BFb group had improved significantly more than the Control group. This process was
234 repeated on an individual level for each participant in the BFb group to assess if their

235 individual responses were significantly better than the Control group. This group and
236 individual process for $Coord_{Var}$ was repeated for Performance variability ($Perf_{Var}$) using $Perf_{Var}$
237 gradients ($PV_{Gradient}$), where $Perf_{Var}$ was quantified as the coefficient of variation (standard
238 deviation divided by the mean x 100) of the peak horizontal CoM velocity (calculated as
239 horizontal impulse divided by mass, with initial CoM velocity at F_0 of $0\text{ m}\cdot\text{s}^{-1}$).

240

241 **3 Results**

242 *3.1 Changes in kinematics*

243 The session of the breakpoint (S_{BP}) was identified to occur within the second visit for all three
244 joints in the BFb group (block 9, 8 and 8 for hip, knee and ankle joints respectively; figure 5)
245 and not to occur at all for the Control group. At S_{BP} the BFb group kinematics (mean \pm 95%CI:
246 hip $42 \pm 23\%$; knee $29 \pm 12\%$; ankle $31 \pm 24\%$) were also significantly greater than for the
247 Control group (hip $8 \pm 10\%$, $p=0.007$; knee $-5 \pm 9\%$, $p<0.001$; ankle $-1 \pm 12\%$, $p=0.014$).
248 Following S_{BP} , at the retention visits, the BFb participants retained significantly greater peak
249 extension angular velocities (Table 1; $p<0.05$). Further, for all three joints and all three
250 retention visits the 95%CI for the BFb were greater than the pre-intervention of 0% indicating
251 that the BFb group were able to retain the kinematic changes induced by the BFb conditions
252 throughout the 26 weeks. In contrast, the Control group 95%CI all encompassed 0% indicating
253 that no learning had occurred.

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257 **Table 1.** Peak extension angular velocity for the hip, knee and ankle joints at each of the
 258 retention visits at weeks 4-6 ($Retention_{Wk4-6}$), 13 ($Retention_{Wk13}$) and 26 ($Retention_{Wk26}$). Data are
 259 percentage change from pre-intervention, and are means \pm 95%CI. The 2x3 mixed ANOVA main
 260 effects and interaction are provided for each joint.

261 * Signifies significant difference from pre-intervention ($p < 0.05$)

262 † Signifies significant difference between BFb and Control groups ($p < 0.05$)

Joint	Visit	BFb group	Control group	Statistics	<i>p</i>
Hip	$Retention_{Wk4-6}$	30 \pm 18*	5 \pm 18	Group main effect	0.024†
	$Retention_{Wk13}$	39 \pm 23*	-2 \pm 22	Time main effect	0.590
	$Retention_{Wk26}$	35 \pm 21*	7 \pm 20	Interaction	0.095
Knee	$Retention_{Wk4-6}$	24 \pm 11*	-7 \pm 11	Group main effect	0.001†
	$Retention_{Wk13}$	24 \pm 11*	-4 \pm 10	Time main effect	0.094
	$Retention_{Wk26}$	25 \pm 11*	0 \pm 11	Interaction	0.274
Ankle	$Retention_{Wk4-6}$	27 \pm 20*	-7 \pm 20	Group main effect	0.027†
	$Retention_{Wk13}$	32 \pm 23*	-3 \pm 23	Time main effect	0.972
	$Retention_{Wk26}$	34 \pm 23*	0 \pm 23	Interaction	0.120

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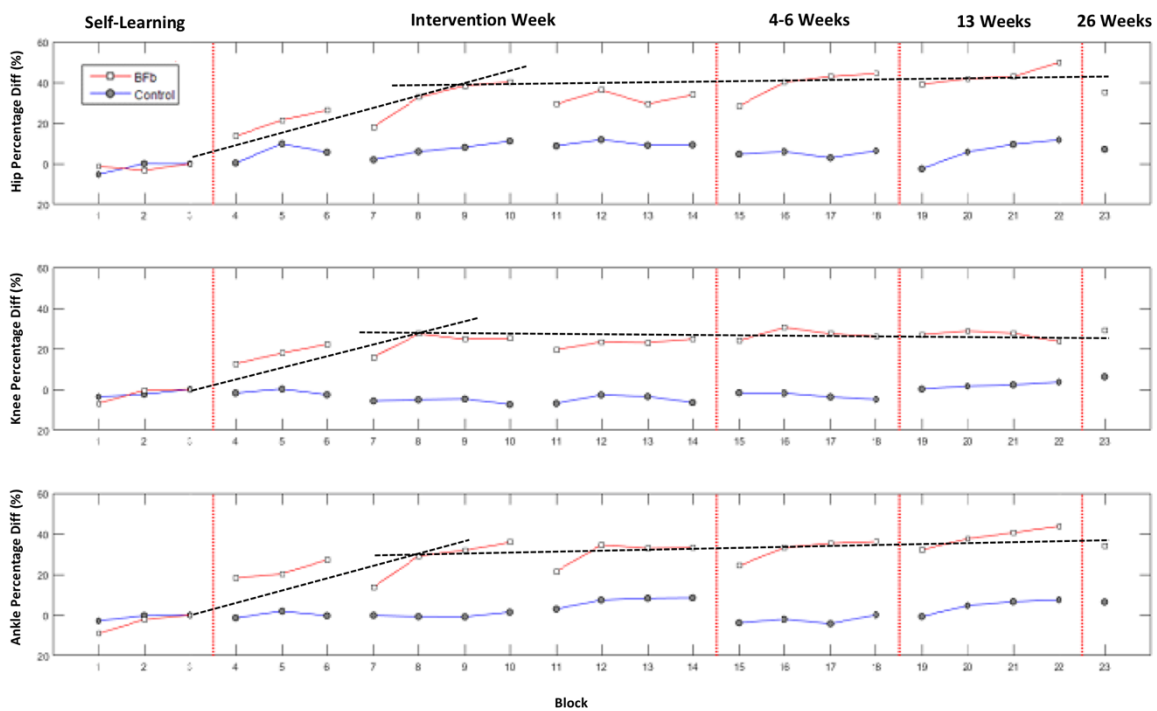
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275 **Figure 5.** Mean percentage change of joint angular velocities for biofeedback (BFb) and
 276 Control groups (0% at block 3). Each shape represents one block. The red vertical dashed lines
 277 separate sessions (Self learning, Intervention, 4-6 Weeks, 13 Weeks and 26 Weeks). Black
 278 dashed lines represent simple piecewise linear regressions, and the breakpoint (S_{BP}) in the
 279 regression lines indicate where learning changes from increasing to plateauing occurring in
 280 session 2.

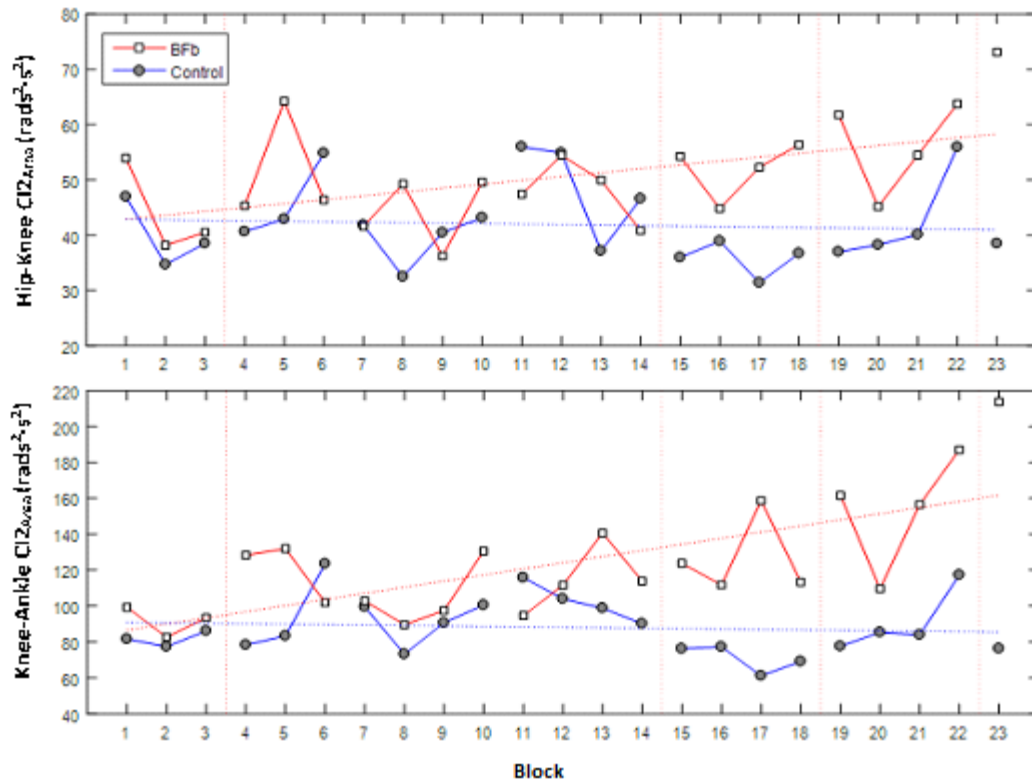


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282 3.2 Changes in Coordination Variability

283 The BFb group showed a continual increase in $CI2_{Area}$ over time in both the hip-knee ($CV_{Gradient}$;
 284 BFb = 0.7 versus Control = -0.9), and knee-ankle $Coord_{Var}$ ($CV_{Gradient}$; BFb = 3.14 versus Control
 285 = -0.24) versus decreases in the Control group (figure 6). The increase in variability in the BFb
 286 group did not plateau over time. Group $Perf_{Var}$, as a measure of task performance variability,
 287 was unchanged over the 6-months in both groups ($PV_{Gradient}$; BFb = -0.01 versus Control =
 288 0.00).

289 **Figure 6.** Hip-knee (top) and knee-ankle (bottom) coupling coordination variability ($CI2_{Area}$)
 290 profiles for biofeedback (BFb) and Control groups over 23 blocks, spanning 26 weeks. The
 291 vertical red dashed lines separate between sessions (Self learning, Intervention, 4-6 weeks, 13
 292 weeks and 26 weeks). Dashed lines are simple linear regressions fitted to each group.



301 On an individual level, for hip-knee $Coord_{Var}$ 7 out of 15 BFb participants and for knee-ankle
 302 $Coord_{Var}$ 8 BFb participants showed significantly greater increases throughout the reduced
 303 schedule biofeedback intervention relative to the Control group (Table 2). In contrast, $Perf_{Var}$
 304 did not alter over time for most participants, with only two of the BFb group's $PV_{Gradient}$
 305 exceeding the Control group's $95\%CI_{Gradient}$ (lower bound, -0.11; upper bound, 0.12).

306 **Table 2.** Individual changes in coordination variability gradients (CVGradient) determined
 307 from coordination variability (CI2Area) for BFb group hip-knee and knee-ankle couplings.

308 *Signifies BFb individuals with CVGradient greater than Control group's 95%CI upper bound of
 309 their CVGradient.

		Hip-Knee CV _{Gradient}		Knee-Ankle CV _{Gradient}	
	BFb Participant #	Control	BFb	Control	BFb
310					
311	1	0.26	5.13*	-0.19	18.97*
312	2	0.09	0.54	0.05	10.39*
	3	0.39	1.58*	1.43	1.64
313	4	-0.17	0.49	-0.15	-3.46
	5	-0.11	-0.81	-0.88	-1.05
314	6	0.95	-0.10	3.28	-1.51
	7	-1.94	1.58*	-7.90	12.54*
315	8	-0.12	1.26*	1.44	-0.56
	9	1.33	2.24*	-0.12	4.97*
316	10	-0.43	-0.06	-0.62	3.40*
	11	-1.46	-1.62	-3.49	-3.53
317	12	-0.54	-0.02	0.29	-1.56
	13	-0.37	1.62*	3.34	6.37*
318	14	-0.05	-0.80	-1.42	1.83*
	15	1.67	1.34*	0.54	7.80*
319	Control Group	95%CI Upper	1.21	95%CI Upper	1.72
320		95%CI Lower	-0.79	95%CI Lower	-0.07

321

322

323 4 Discussion

324 Addressing the first aim to identify when changes in directly targeted BFb variables occurred,
 325 the breakpoint analysis on hip, knee and ankle angular velocity changes shows that the visual
 326 feedback design used in this research was effective, with athletes attending to the BFb and
 327 showing a plateau in motor development within just two sessions (figure 5). Kinematic
 328 changes occurring following just one visit of BFb have been shown in both continuous (Crowell
 329 et al., 2010; Baggaleley et al., 2017) and discrete skills (e.g. squatting; Ford et al., 2015).

330 However, without retention testing in these studies it is not possible to confirm that changes
331 were maintained. With changes occurring early on, the present study also highlights that
332 complex BFb information given to participants can encourage changes in technique, but
333 without distracting participants from important sources of internal information (Park et al.,
334 2000). Encoding complex data into a simple presentation, with the addition of transitional
335 information on how to alter performance, helps enhance BFb effectiveness (Kernodle and
336 Carlton, 1992). For all three joints' peak extension angular velocities, the Control group did
337 not change from pre-intervention to any of the three retention visits ($p>0.05$). In contrast, the
338 BFb group significantly improved by the Retention_{Wk4-6}, and this improvement remained for
339 the further Retention_{Wk13} and Retention_{Wk26} visits ($p<0.05$). This improvement in the BFb
340 group shows that the kinematic changes induced were relatively permanent. This learning
341 supports that there was no dependency from a reducing BFb schedule where BFb was
342 delivered with ever increasing time between visits. A reducing schedule is thought to foster
343 cognitive strategies through mental rehearsal, with sufficient time between visits enhancing
344 cognitive processing (Thorpe and Valvano, 2002). Intelligent BFb scheduling, paired with a
345 reducing schedule, may therefore be an effective method in the long term to avoid
346 dependency effects of BFb while still allowing a large volume of information to be used to
347 induce specific changes in a complex skill.

348 The skill adaptations shown within just two sessions highlight how effective knowledge of
349 performance BFb can be when used appropriately. The feedback specifically guides an
350 individual on how to achieve a desired movement related to their performance, which is
351 increasingly important when a specific technique is the focus of an intervention. Allowing a
352 system to self-organise rather than defining constraints (e.g. kinematic patterns) may be more

353 useful in some cases, such as in novice motor learning (e.g. Wulf et al., 2010), however not
354 necessarily as beneficial when attempting to direct specific movement patterns as in
355 rehabilitation (e.g. van den Heuvel et al., 2016). Although changes occurred quickly, it is
356 important to consider the influence of BFb on more permanent learning for real world
357 applications, particularly during a reducing BFb paradigm.

358 Addressing the second aim to apply a new measure of $Coord_{Var}$ to explore skill exploration,
359 the results demonstrate that $CI2_{Area}$ was effective in identifying changes in $Coord_{Var}$ of the hip-
360 knee and knee-ankle joint couplings between a Control group and a skill development BFb
361 intervention group. Importantly, these findings were demonstrated in a complex skill
362 involving the whole lower limb, making it potentially applicable to other real-world skills.
363 Using results from $CI2_{Area}$, it can be ascertained that the BFb intervention does indeed guide
364 skill exploration as suggested in previous research (Lauber et al., 2013). The continual increase
365 in $CI2_{Area}$ also highlights the increasing exploration throughout the six-month intervention
366 period, which supports that a reducing BFb schedule does not lead to dependency whereby
367 exploration ceases. Quantification using $CI2_{Area}$ also allows for the mapping of motor learning
368 theory to applied practice. According to Bernstein's (1967) stages of motor learning,
369 participants in this research can be seen continually freeing the coordinated degrees of
370 freedom to explore task execution evidenced by the increasing $Coord_{Var}$. This is also in line
371 with concepts proposed by Newell (1985) in that the BFb group were self-organising hip-knee
372 and knee-ankle joint couplings to satisfy task constraints of the skill in achieving maximal CoM
373 propulsion, but had not fully gained control of the complex motor skill to converge on a stable
374 pattern. In this respect, $CI2_{Area}$ values could be used to indicate when changes to the
375 intervention may have been required to better facilitate the development of a more stable

376 Coord_{Var} pattern. Therefore, perhaps more BFb would have helped to solidify learning,
377 although it is difficult to establish this without using CI2_{Area} results to manipulate schedules
378 mid-intervention. In future, CI2_{Area} could be applied to assess changes of Coord_{Var} in real-time.
379 It can be postulated that the low volume of BFb (six hours per individual) kept BFb participants
380 in a continual state of exploration. However, questions do arise as to when this increase would
381 plateau, or even reduce, as prescribed in Bernstein's (1967) and Newell's (1985) theoretical
382 frameworks. These paradigms both suggest that Coord_{Var} may decrease as a skill is mastered
383 but would still allow functionally variable interactions to maintain a stable and successful
384 performance outcome as seen with Perf_{Var} remaining consistent in both groups. Future
385 research should seek to identify changes of Coord_{Var} using CI2_{Area} in comprehensive, complex-
386 skill, motor learning interventions to provide more comparative data to map learning to
387 stages of learning.

388 Importantly, CI2_{Area} was able to identify the individual responses to the skill intervention. The
389 importance of individualised approaches is evident in clinical practice and high-performance
390 sport (e.g. Needham et al., 2018; Glazier and Mehdizadeh, 2018). Relative to the Control
391 group's hip-knee CI2_{Area} over the six months, 7 out of the 15 BFb group's individual CV_{Gradient}
392 were greater than the Control group's upper 95%CI_{Gradient}. Almost half of the BFb group
393 explored the rear leg propulsion pattern by increasing hip-knee coupling exploration
394 strategies. In addition, 8 out of 15 BFb individuals had knee-ankle coupling CV_{Gradient} which
395 exceeded the upper 95%CI_{Gradient} of the Control group. This is in line with previous research
396 underpinning whole limb sequential coordination strategies, with the more distal joints
397 offering a compensatory strategy for movement errors in more proximal segments (Robins et
398 al., 2006; Mullineaux and Uhl, 2010). Looking at both joint couplings across individuals, the

399 same 5 individuals (Table 2) had both hip-knee and knee-ankle coupling variability greater
400 than the control group. This also seems to suggest that certain individuals have greater
401 $Coord_{var}$, which may be a strategy underpinning motor learning effectiveness and supports
402 the importance of exploring individuals' approaches to skill development.

403

404 **5 Limitations**

405 The main limitation that became apparent following the intervention is how quickly the
406 individuals satisfied the task to cover a distance of 1.5 times leg length. The distance was fixed
407 to maintain scientific control but in future a progression in task complexity should be
408 incorporated. This may have inhibited further increases in performance, as individuals felt the
409 target was too close at the end of the intervention week. This, paired with continually
410 increasing $Coord_{var}$ suggests participants were still exploring the skill over 26 weeks. The joint
411 definitions within this study were chosen as they required a small number of anatomical
412 landmarks which may assist in any future development of BFb devices. However, as these
413 definitions, including that the hip joint definition is a segment definition, may influence the
414 proximo-distal sequencing and $Coord_{var}$ calculations in an undesirable manner. Through BFb
415 there was an increase in both joint angular velocity and $Coord_{var}$, and partitioning out the
416 causal variance component of this relationship needs exploring. Methodologically, $CI2_{Area}$
417 provides a robust measure, however further work is required to verify the validity of whether
418 an increase or decrease in $Coord_{var}$ is reflective of changes in motor learning.

419

420

421

422 **6 Conclusion**

423 Directly targeted kinematic variables can be altered using BFb within just two sessions in a
424 complex, whole limb skill. The use of a longitudinally reducing BFb schedule was effective in
425 avoiding dependency properties of BFb, demonstrated with no significant reduction in skill
426 during retention tests over 26 weeks. A new approach to assess coordination variability using
427 $CI2_{Area}$ was effective in identifying group and individual skill exploration strategies and can be
428 explored in the future to map individual exploration strategies to the stages of motor learning.

429

430 **7 Conflict of Interest Statement**

431 The authors declare that there is no conflict of interest regarding the content of this article.

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